

Dynamic configuration of large-scale cortical networks accounts for heterogeneity in ADHD traits

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Introduction

How do specific **neural mechanisms** manifest at the behavioural level as **distinct ADHD traits** (inattention, hyperactivity/impulsivity)?

Key objective in the dimensional approach to psychopathology outlined by the National Institute of Mental Health¹.

A primary cognitive deficit in those with ADHD is the ability to **execute and inhibit motor responses**², often operationalized through performance on inhibitory control tasks (i.e, Go/NoGo). Some evidence suggests individual differences in the neural mechanisms underlying this ability specifically account for **hyperactivity/impulsivity**:

1) Methylphenidate, known to supress task-irrelevant connectivity, is more effective at reducing hyperactive/impulsive than inattentive traits 3,4

2) White matter tract abnormalities **connecting regions in the frontal and motor cortex** (involved in motor response execution/inhibition) are prominent in **ADHD-C**⁵

However, these mechanisms are not always prominent sources of ADHD heterogeneity:

1) Regional neural activity suggest motor inhibition is intact 6

2) Cognitive measures of execution/inhibition often fail to differentiate subtypes 7.8.5

Perhaps the *dynamic changes* that large-scale cortical networks undergo during motor response/execution differ between ADHD subtypes traits.

If this is the case, then graph-theoretical measures which capture how EEG functional networks dynamically organize during motor response execution/inhibition should reliably distinguish between ADHD traits (Inattention, Hyperactivity/Impulsivity).

Methods

Participants • 62 non-clinical participants (ages 18-24; 32 male) • ADHD traits assessed using Conner's Adult ADHD Rating scales.

<u>EEG</u>

- Continuous 128-Channel EEG (500Hz Sampling rate).
 Preprocessing: 100Hz low pass, 60Hz notch, .5Hz high pass filter
 Ocular correction: Gratton & Coles.
- Artifact Rejection: Trials with amplitude +/-200uV rejected.
- Signal filtered (1-3Hz; 4-7Hz; 8-13Hz; 14-29Hz; 30-90Hz), and phase time-series extracted using Hilbert transform.
- Across-trial Phase-lag Index (PLI) used to measure connectivity (synchronization between signals).
 EEG Functional Networks constructed: 'Edges' = PLI (connectivity); 'Nodes' = electrodes.
 Dynamic Networks: Sensor X Sensor adjacency matrices over time (2ms; temporally layered).
 Static Networks: Sensor X Sensor adjacency matrices averaged over 0-500ms

Task

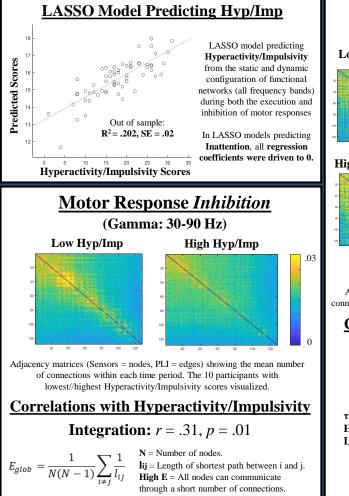
A-X Continuous performance task, Go/No-Go.

- Instructions: "Respond quickly and accurately to X, but only when it is preceded by A."
- Motor Response *Execution* = Response trials: 42.18/subject.
- Motor Response Inhibition = No response trials: 44.35/subject.

LASSO Regression

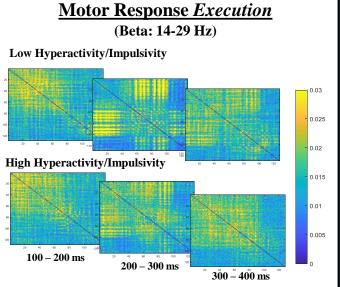
Least absolute shrinkage and selection operator (LASSO) regression used to predict ADHD traits.
 Features: Ten dynamic/static network measures (broadly capturing modularity, small-worldness, integration and segregation) for each frequency-band and both conditions (100 features per model).
 Outcome Variables: CAARS-Inattention, CAARS-Hyperactivity/Impulsivity
 Ouroffitting anymented by calculate hyperactivity law plant through reported 10 feld areas validation

• Overfitting prevented by selecting hyperparameter lambda through repeated 10-fold cross validation.



Small-Worldness: *r* = .43, *p* = .0006

 $SWI_{stat} = \frac{E_r}{E} - \frac{C}{C_l} \begin{cases} E = \text{Global efficiency: integration.} \\ C = \text{Clustering coefficient: segregation.} \\ r = \text{Random network with equivalent degree.} \\ I = \text{Lattice network with equivalent degree} \\ \text{High SWI} = \text{Greater integration than expected} \\ \text{based on the level of segregation.} \end{cases}$



Adjacency matrices (Sensors = nodes, PLI = edges) showing the mean number of connections within each time period, 10 participants with low//high Hyp/Imp visualized

Correlations with Hyperactivity/Impulsivity

Burstiness: *r* = -.32, p = .017

 τ = Distribution of inter-contact times between all node-pairs. **High B** = Serially correlated communication (distinct on/off periods). **Low B** = Periodic communication (regular intervals).

Modularity:
$$r = .30, p = .018$$

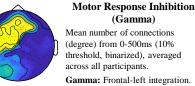
$$Q = \frac{1}{2E} \sum_{ij} (A_{ij} - e_{ij}) \delta(m_i, m_j)$$

 $\mathbf{E} =$ Number of edges.

e = Equivalent random network.

 δ (mi, mj) = Kronecker delta function: equal to 1 if nodes *i* and *j* belong to the same module. High **Q** = Easily divided into distinct 'subnetworks'.

Topography of Effects





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Conclusion

• The dynamic reconfiguration that large scale functional brain networks undergo during motor response execution/inhibition is altered in those with hyperactive/impulsive, but not inattentive, traits. Hyperactivity/Impulsivity is associated with... • During motor response execution: · A modular configuration, with less burst-like integration between modules in networks oscillating at a **beta** frequency. Reflects an altered integration between prefrontal and motor areas. During motor response inhibition: • A more small-world like, integrated configuration in networks oscillating at a gamma frequency. • Reflects a compensatory, integrative

mechanism used to overcome an **under**specialized functional network configuration.

 The neural mechanisms underlying ADHD subtype heterogeneity can be measured by applying network measures to the EEG recorded during a Go/No-Go task, furthering EEG's use in clinical ADHD research.



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